



# Picosecond Avalanche Amorphous Selenium Detector

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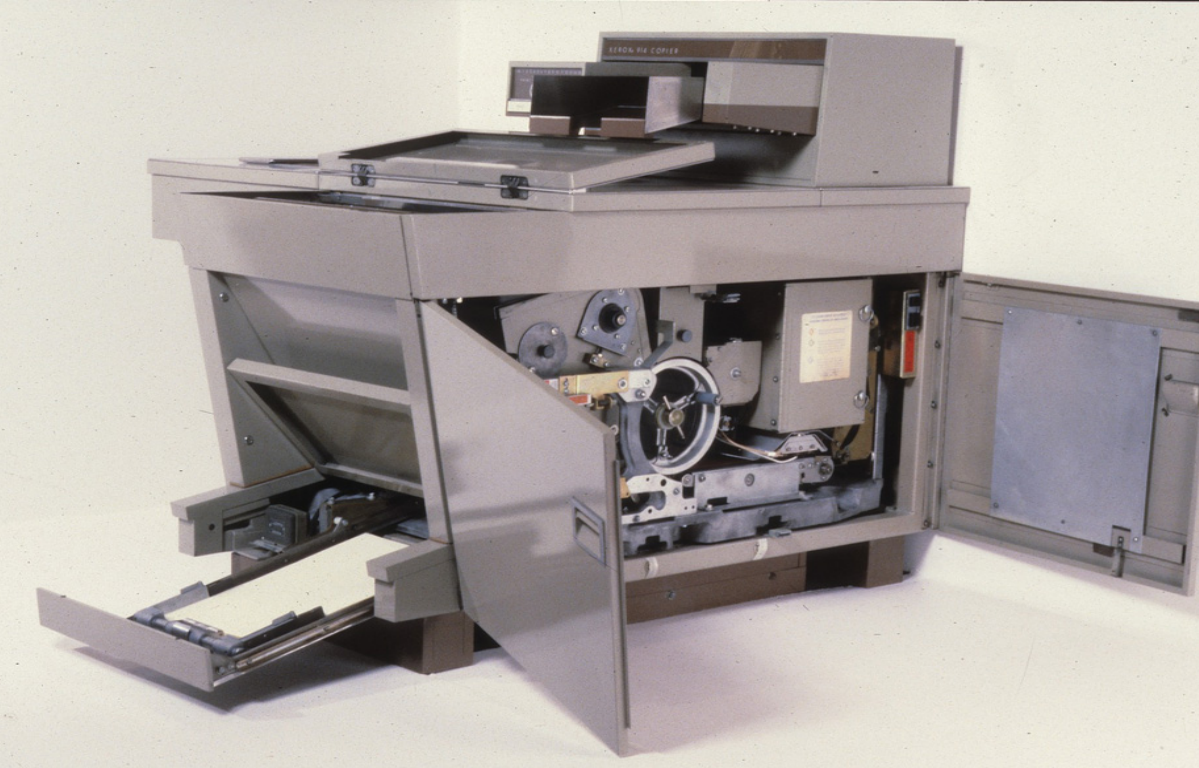
Stony Brook University

- **Amorphous Selenium Inventions**
- **Unipolar Time-Differential (UTD) charge sensing**
- **Multi-Well Selenium Detectors (SWAD, NEW-HARP)**

10.-22.-38

ASTORIA

- **1938:** Chester Carlson invents a method of transferring images from one piece of paper to another using static electricity, a process dubbed xerography.
- **1947:** Haloid gets exclusive right to Carlson's patent.
- **1949:** Company introduces the XeroX Copier.
- **1958:** Company changes its name to Haloid Xerox Inc.
- **1959:** Introduction of the Xerox 914, the first automatic, plain-paper copier, proves to be a huge success.



# Xerography with Selenium

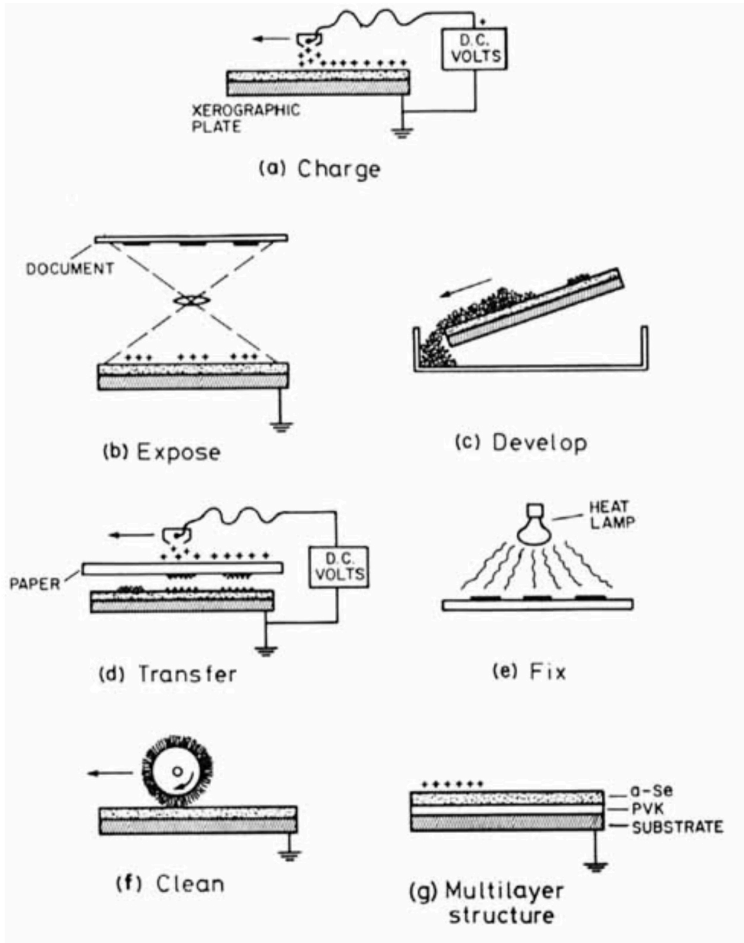
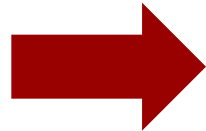
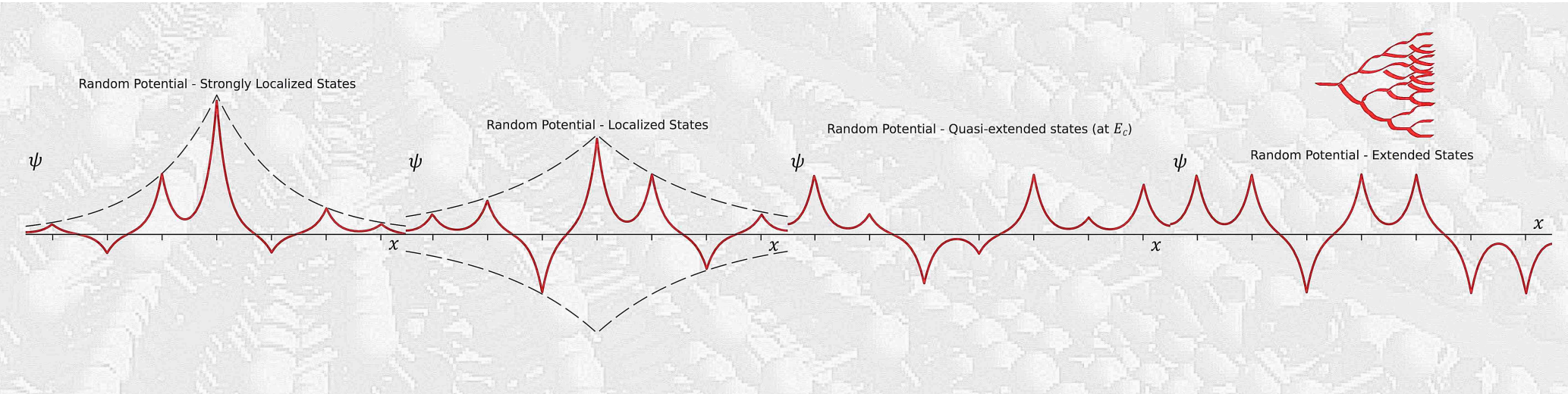


Fig. 2. Basic steps in xerography.

# High Resolution X-ray Imaging



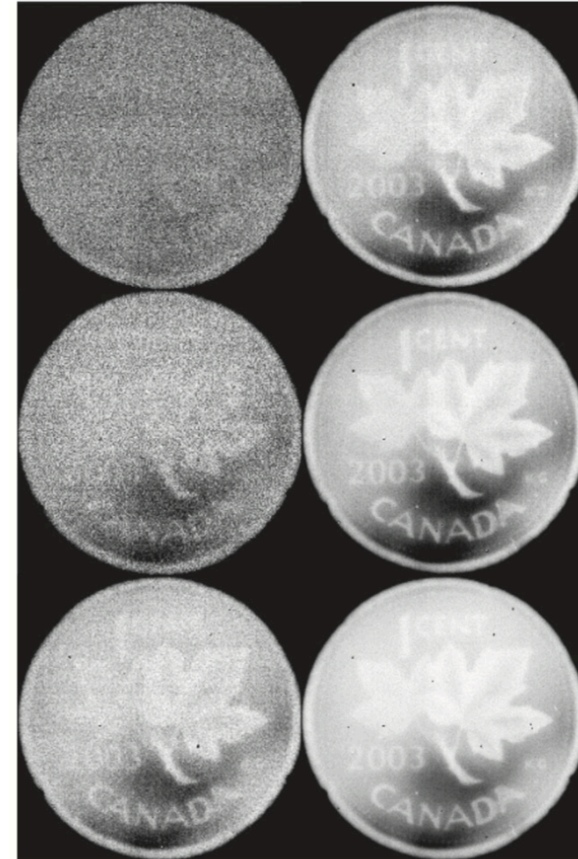
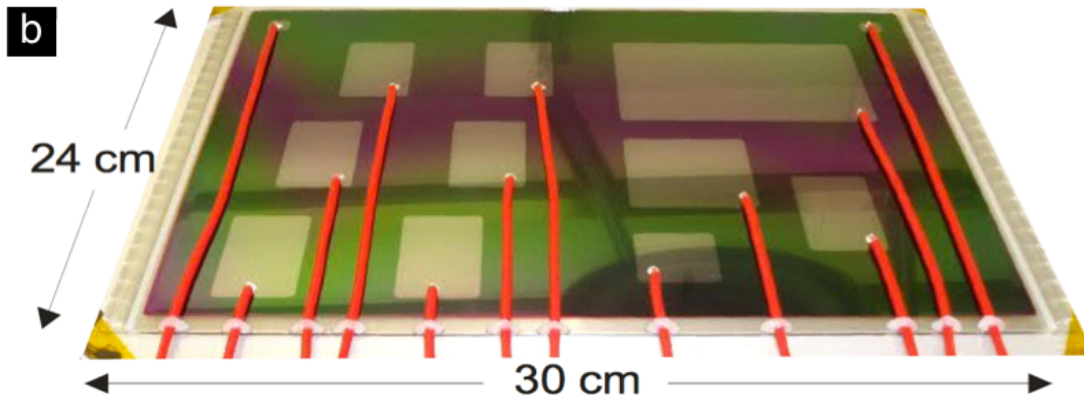
Courtesy of **Analogic Canada.**  
([www.analogic.com](http://www.analogic.com))



Courtesy of **NHK Japan**  
 (Inventor: Dr. Kenkichi Tanioka)

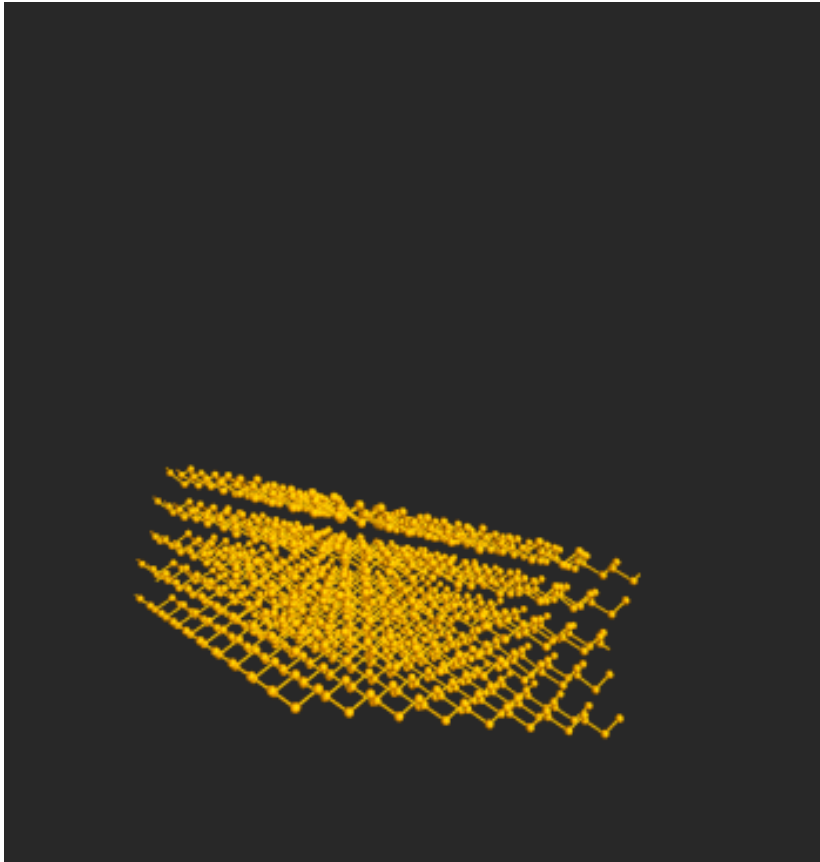


Developed by **W. Zhao's Group**:  
(<https://you.stonybrook.edu/drill/>)

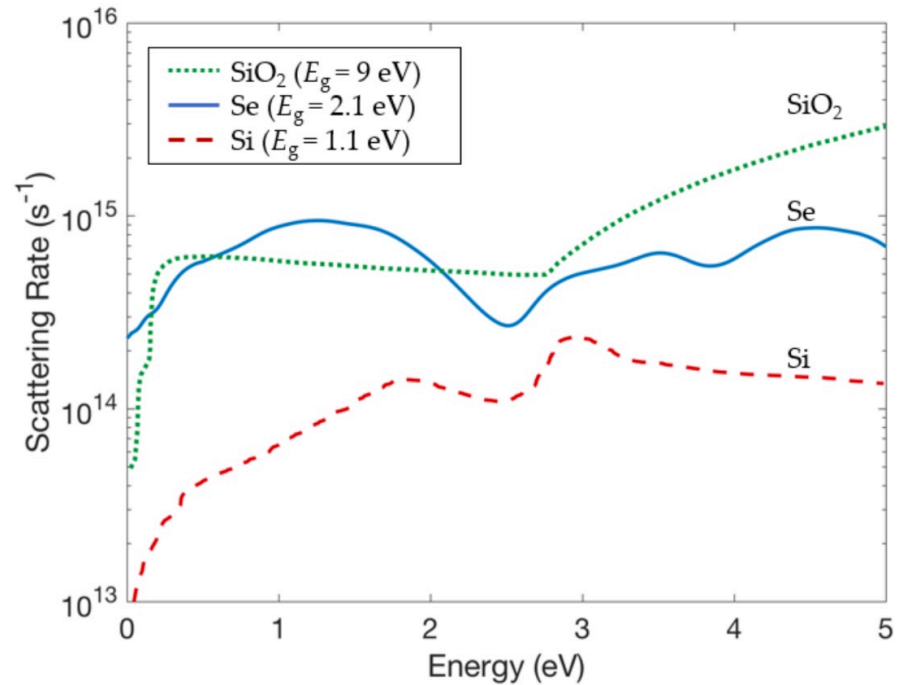


J. R. Scheuermann, A. H. Goldan et al, *Med. Phys.* **42**, 1223-1226 (2015)  
J. R. Scheuermann, A. Howansky et al, *Med. Phys.* **45**, 794-802 (2018).

FIG. 8. Images of the tails side of a penny with constant 0.76 mR exposure. Left column from top to bottom  $E_{Se} = 15, 71, \text{ and } 95 \text{ V } \mu\text{m}^{-1}$ . Right column from top to bottom  $E_{Se} = 95, 100, \text{ and } 105 \text{ V } \mu\text{m}^{-1}$ .



$$\frac{\partial f_{\mathbf{k}}(\mathbf{r})}{\partial t} = -\mathbf{F} \cdot \nabla_{\mathbf{p}} f_{\mathbf{k}}(\mathbf{r}) + \left. \frac{\partial f_{\mathbf{k}}(\mathbf{r})}{\partial t} \right|_{\text{coll}} - \frac{1}{\hbar} \frac{\partial E_{\mathbf{k}}}{\partial \mathbf{k}} \cdot \nabla_{\mathbf{r}} f_{\mathbf{k}}(\mathbf{r}) + s(\mathbf{r}, \mathbf{p}, t),$$

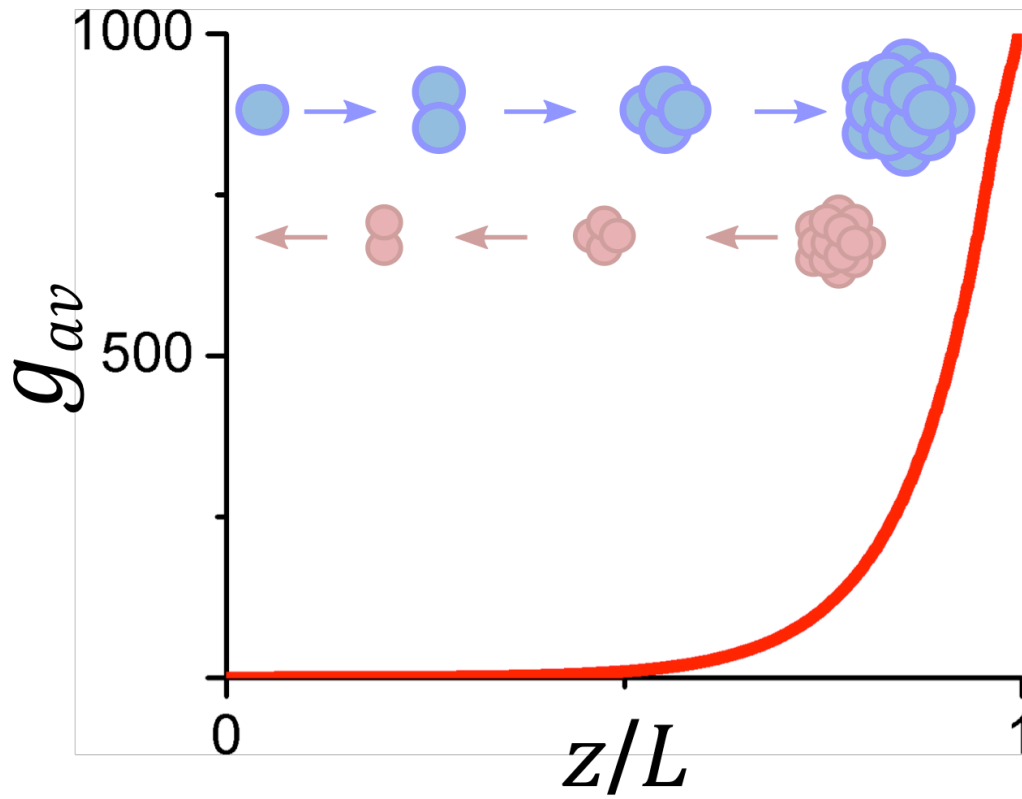


A. H. Goldan *et al*, *J. Appl. Phys.* **120**, 135101 (2016).

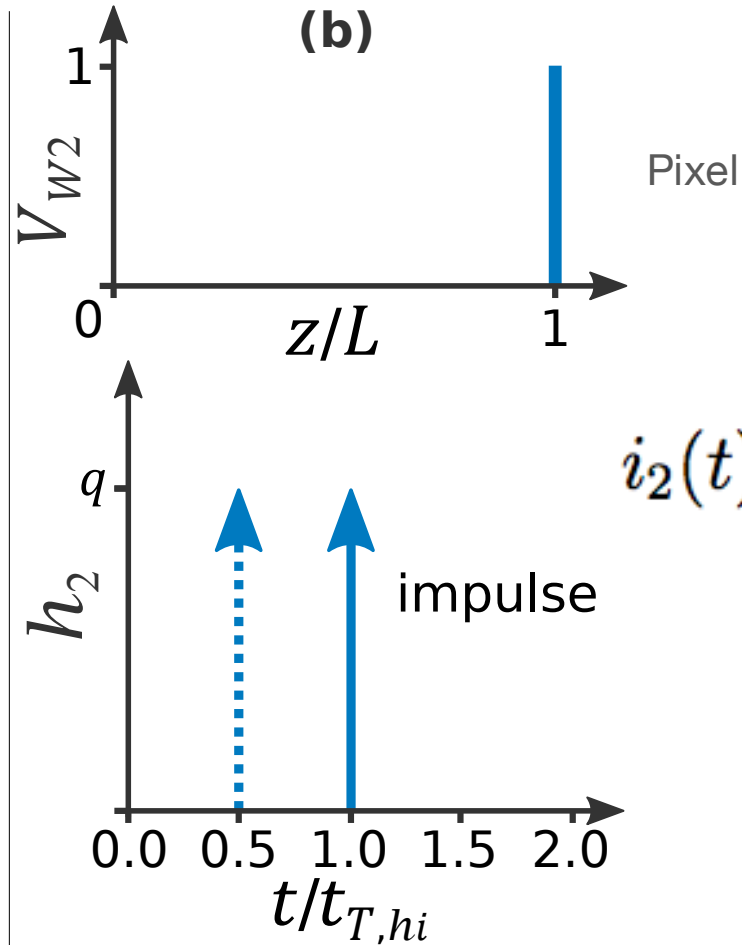
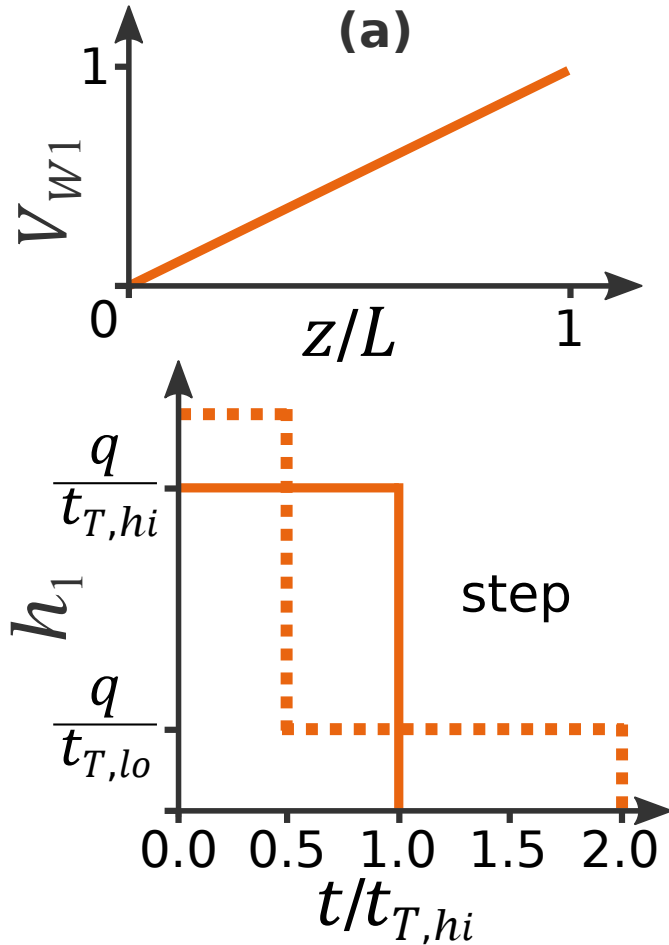
A. Mukherjee, D. Vasileska, A. H. Goldan, *J. Appl. Phys.* **124**, 025846 (2018).

	<b>Modality</b>	<b>Energies</b>
<b>X-ray imaging</b> <i>transmission</i>	Mammography	25 kVp, ~18 keV
	Radiography (chest)	150 kVp
	Fluoroscopy	150 kVp
	X-ray CT	150 kVp
<b>Nuclear Medicine</b> <i>emission</i>	Scintigraphy	80 – 140 keV
	SPECT	60 – 511 keV
	PET	511 keV

# Avalanche Gain in a-Se: Slow Collection

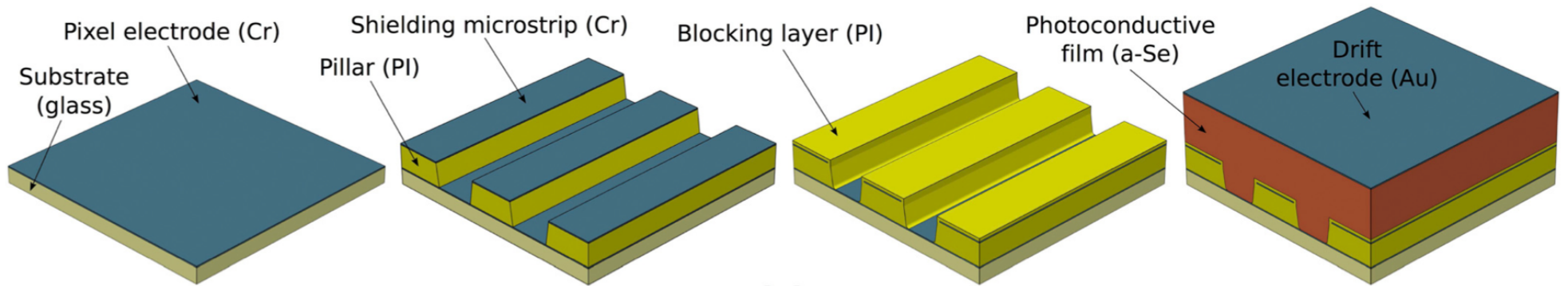


# Unipolar Time-Differential (UTD) sensing

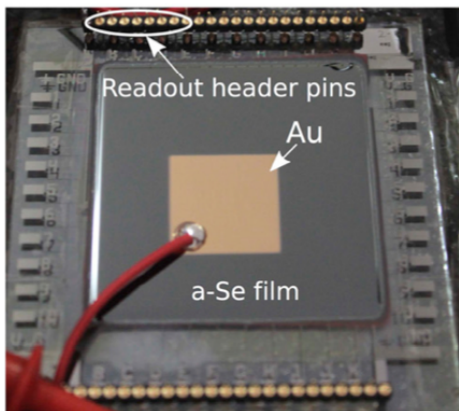


$$i_2(t) = -t_{T,hi} \frac{d}{dt} i_1(t)$$

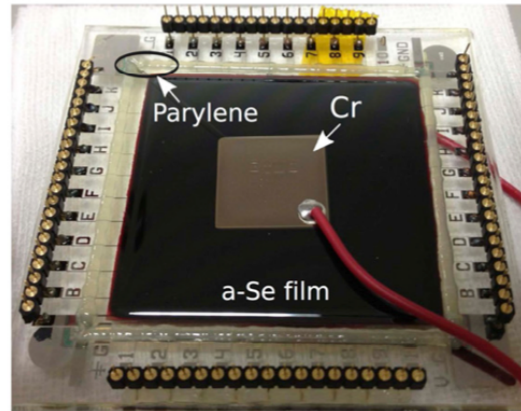
# Multi-Well Detectors



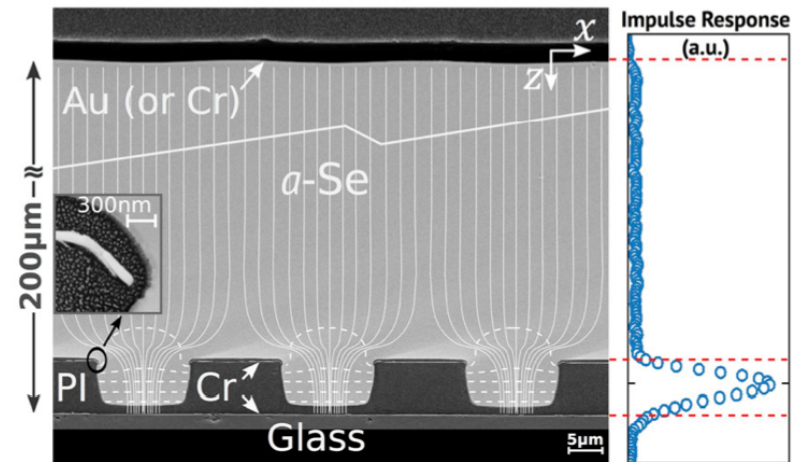
(a)



(b)

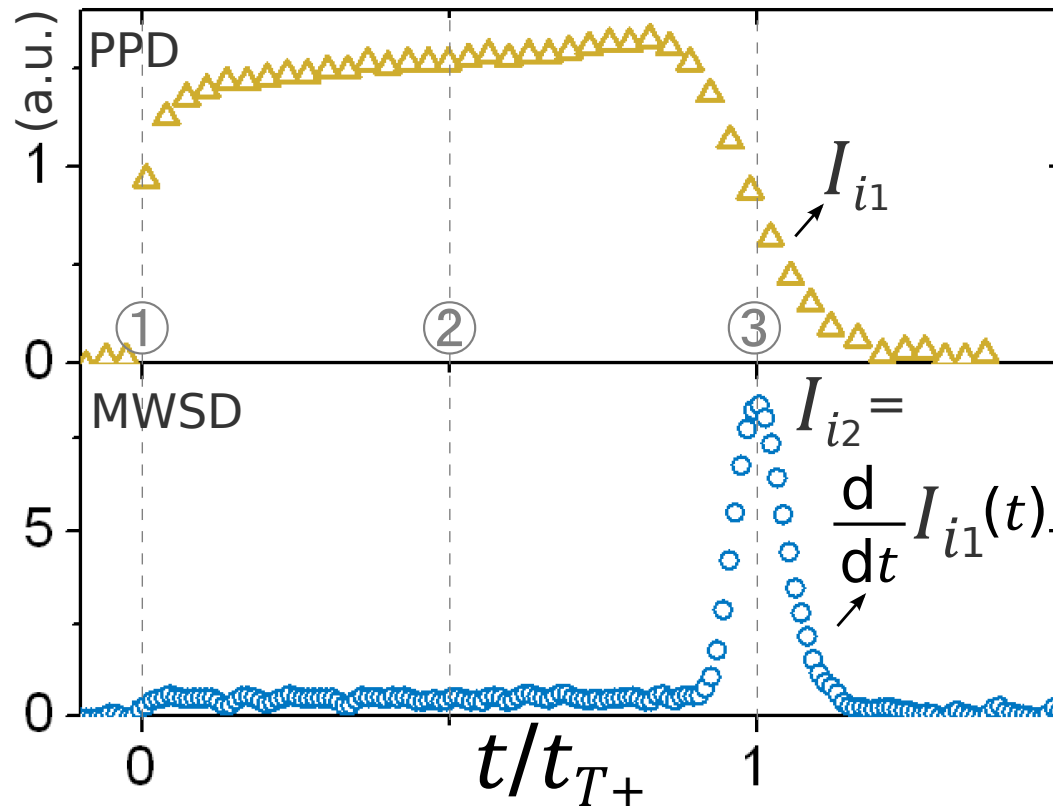


(c)



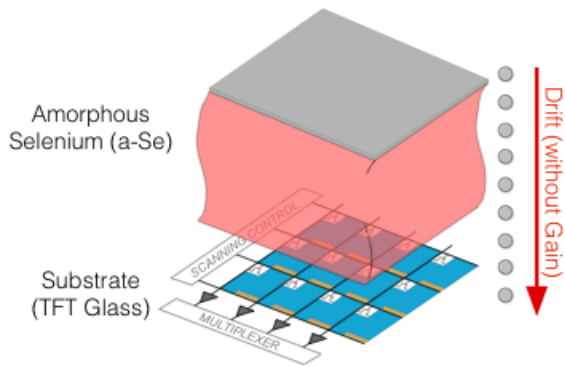
(d)

Excitation = 5ns laser pulse tuned to  $\lambda=337\text{nm}$ .

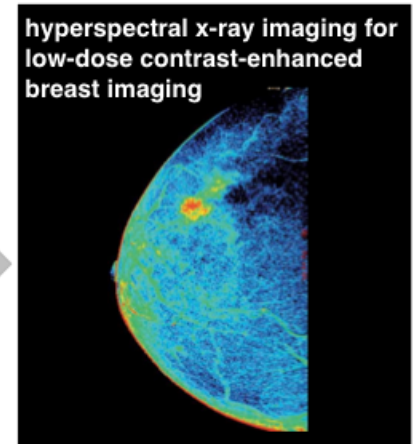
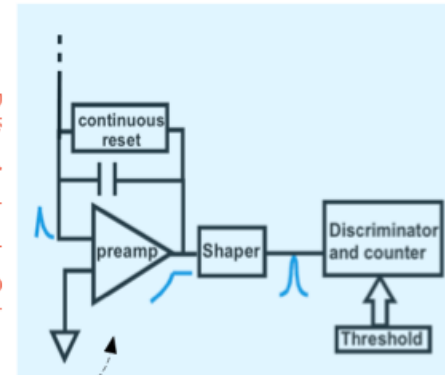
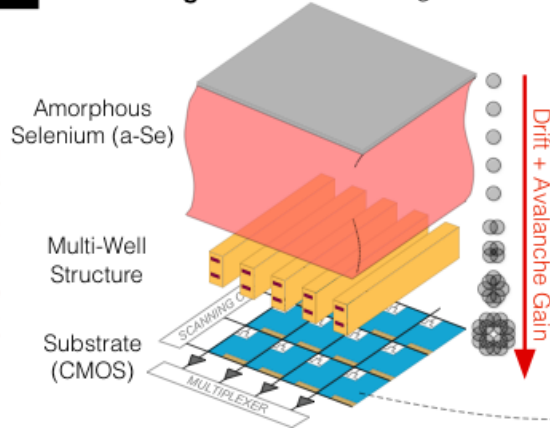


# X-ray Photon Counting Detectors

**a** Planar a-Se Imager: Energy Integration



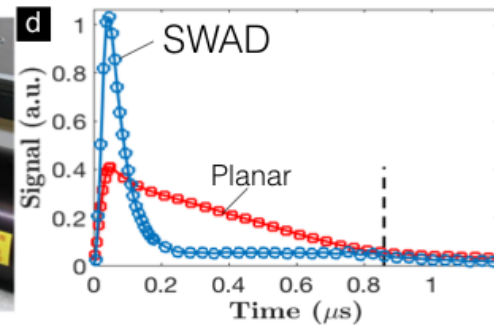
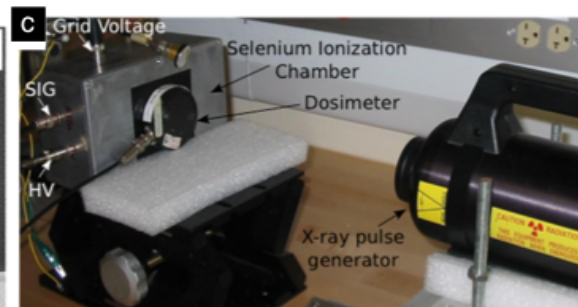
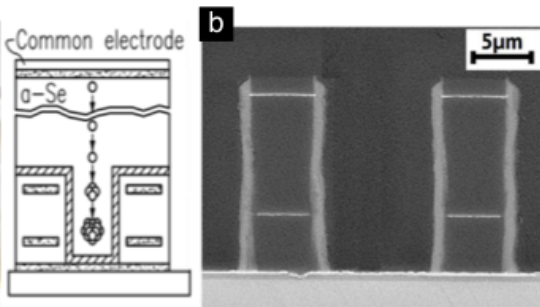
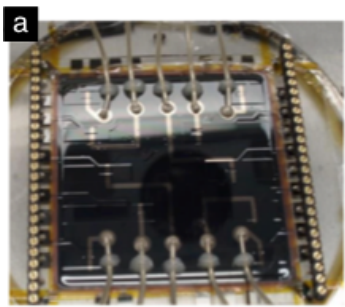
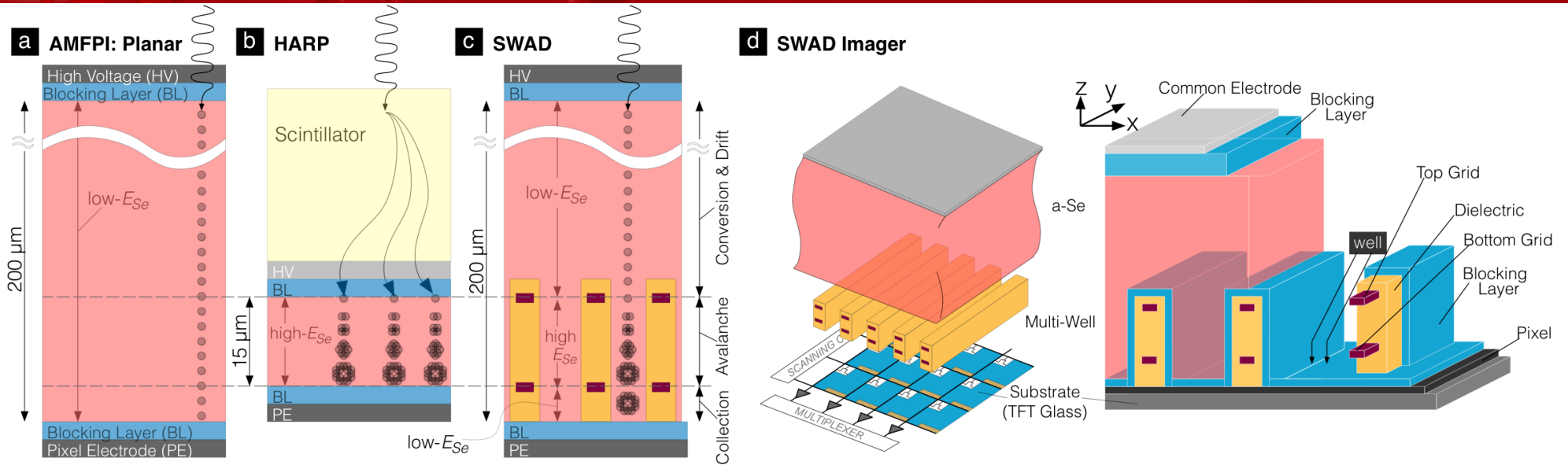
**b** SWAD Imager: Photon Counting



J. Stavro, A. H. Goldan and W. Zhao, *J. Med. Imag.* **5**, 043502 (2018).  
 A. H. Goldan, W. Zhao, *Med. Phys.* **40**, 010702 (2013).

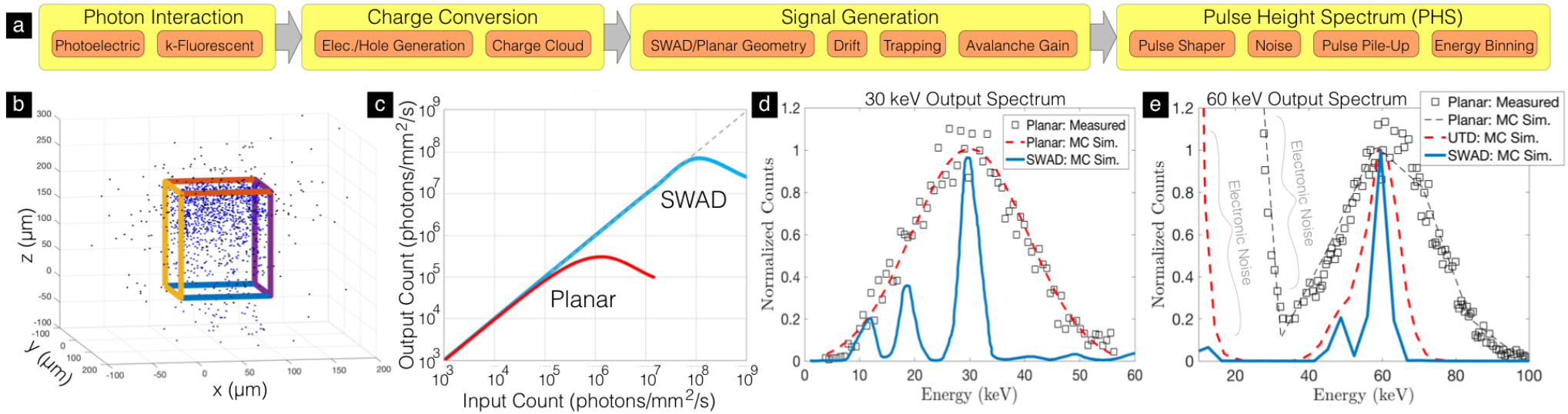


# SWAD: field-Shaping multi-Well Avalanche Detector



J. Stavro, A. H. Goldan and W. Zhao, *J. Med. Imag.* **5**, 043502 (2018).

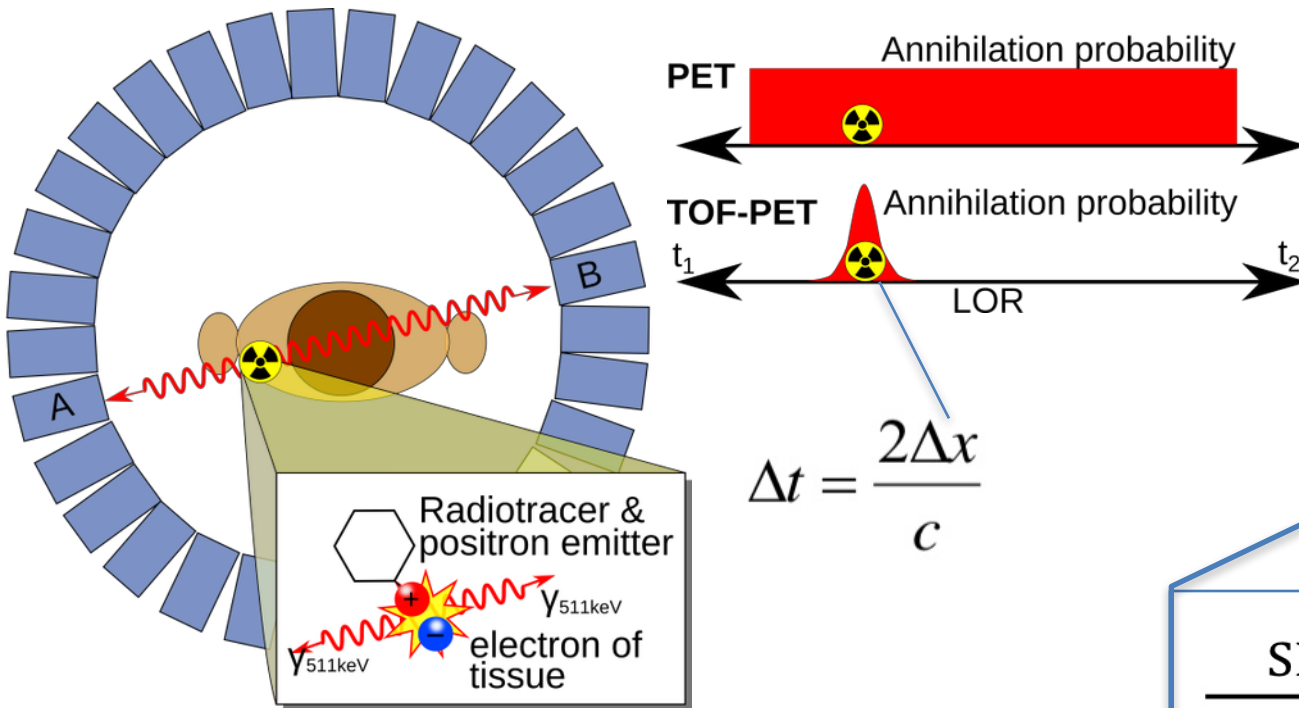
A. H. Goldan, W. Zhao, *Med. Phys.* **40**, 010702 (2013).



J. Stavro, A. H. Goldan and W. Zhao, *J. Med. Imag.* **5**, 043502 (2018).  
 J. Tanguy et al, *Proc. SPIE* **10573**, 105734V (2018).

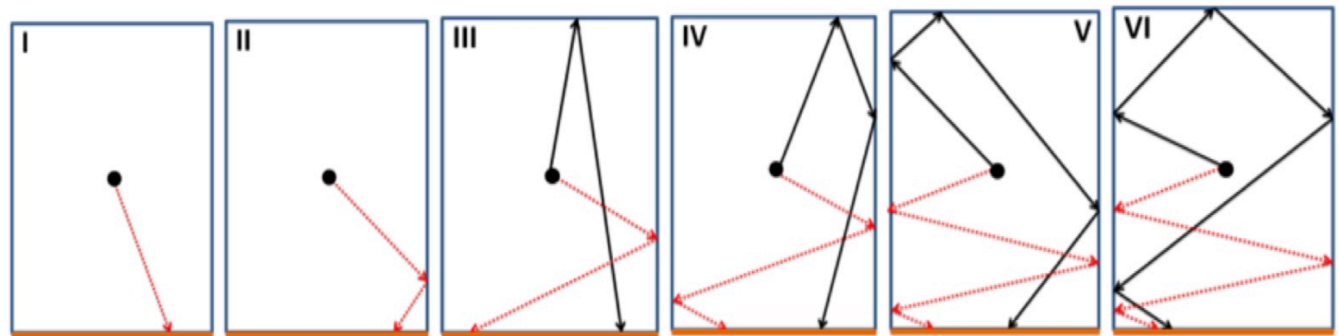
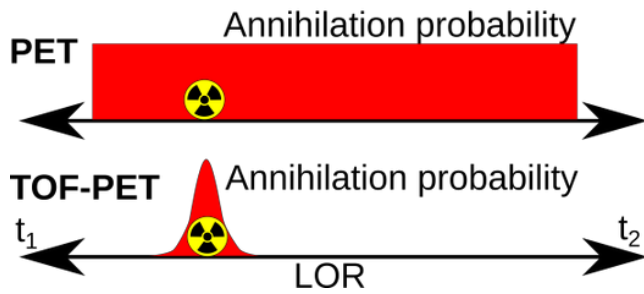
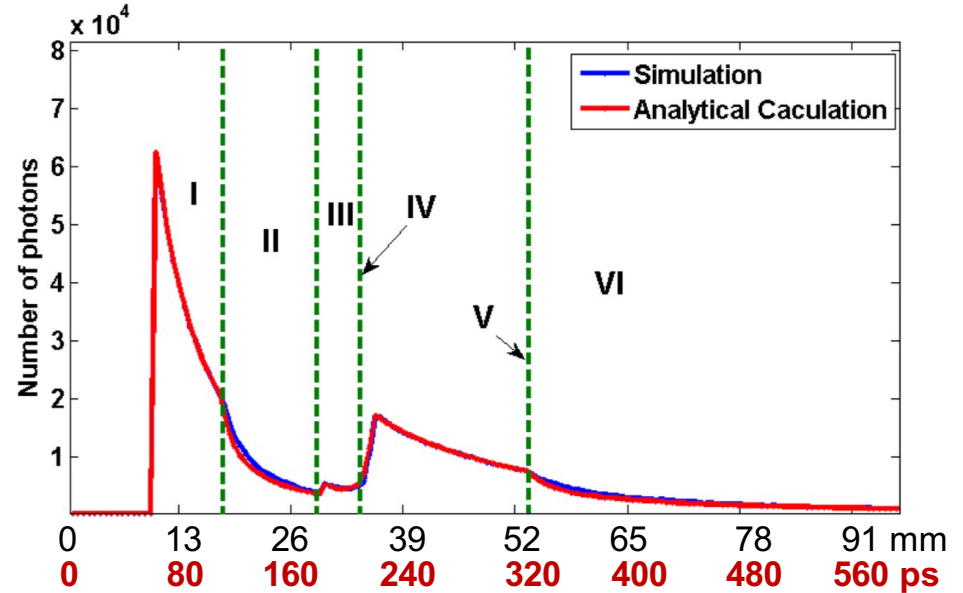
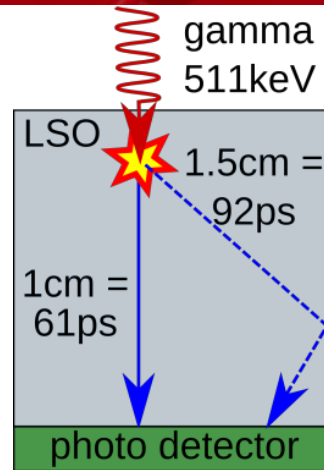
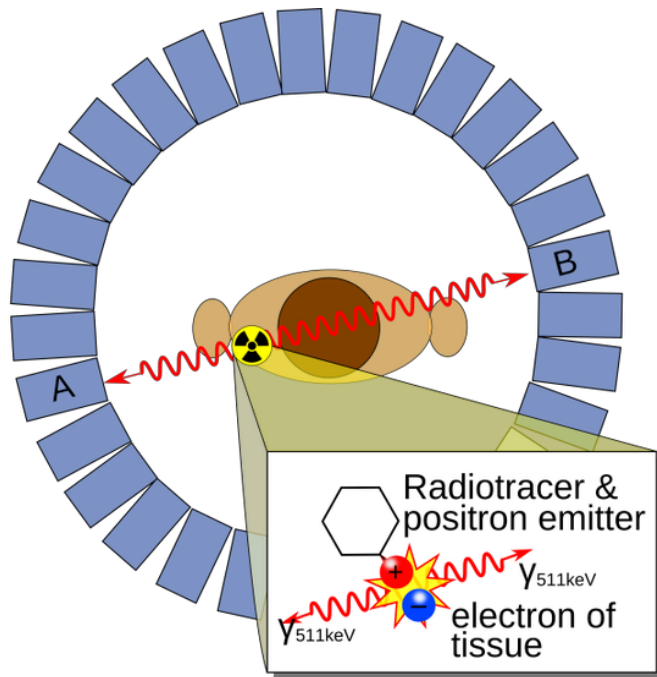
	<b>Modality</b>	<b>Energies</b>
<b>X-ray imaging</b> <i>transmission</i>	Mammography	25 kVp, ~18 keV
	Radiography (chest)	150 kVp
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<b>Nuclear Medicine</b> <i>emission</i>	Scintigraphy	80 – 140 keV
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# Time-Of-Flight (TOF) PET

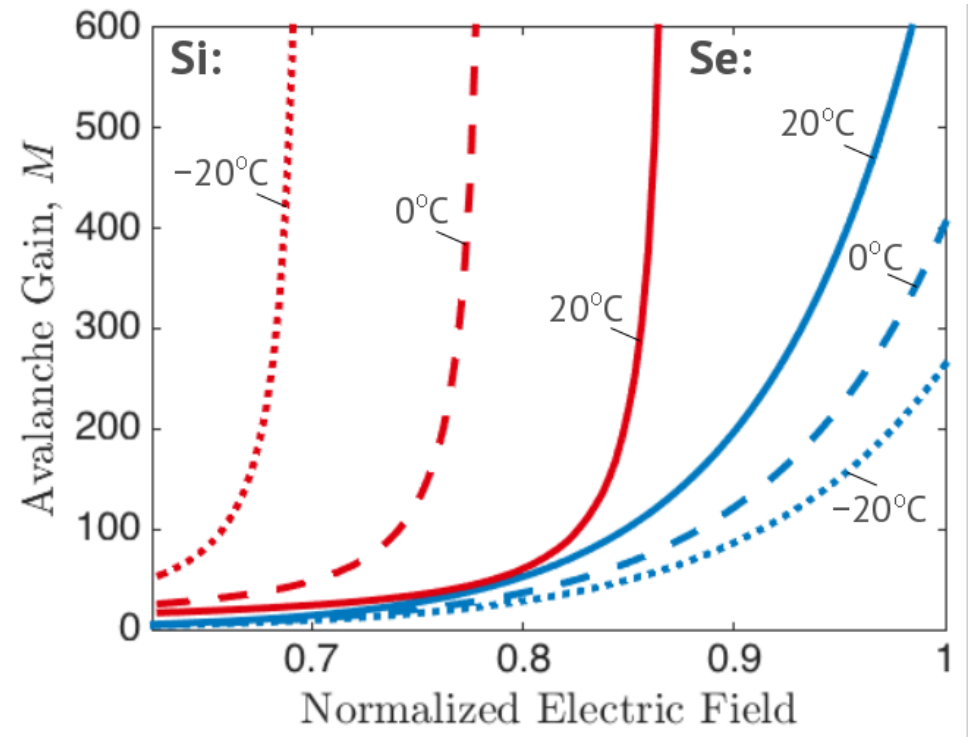
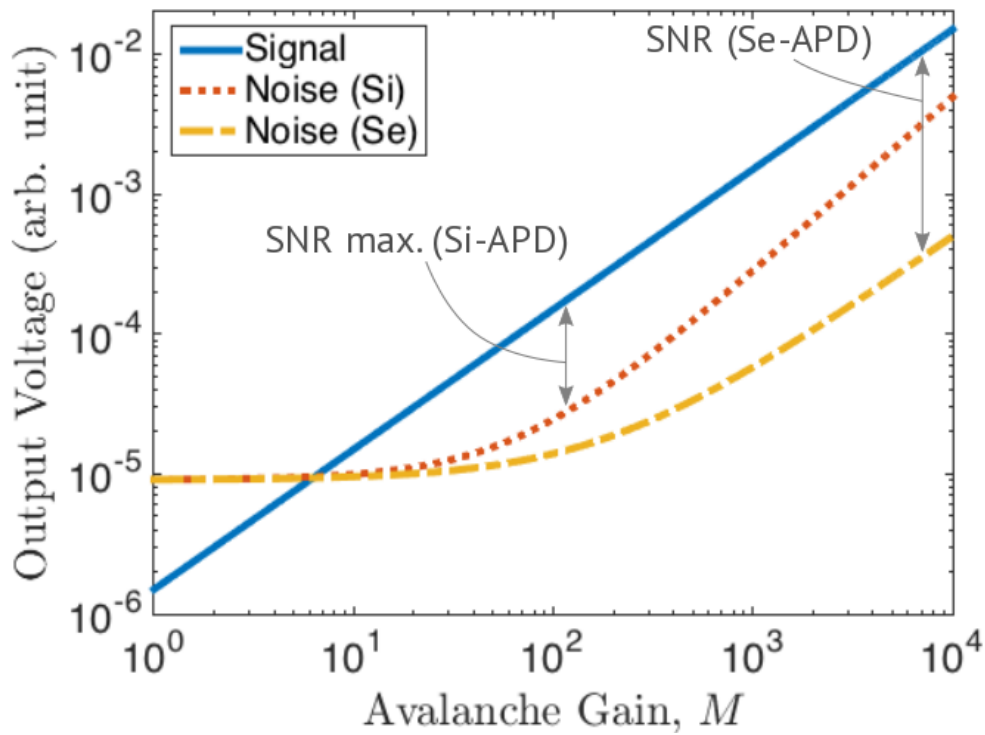


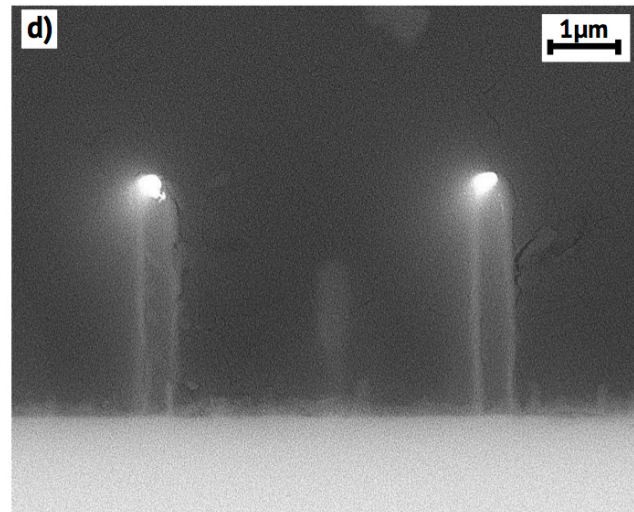
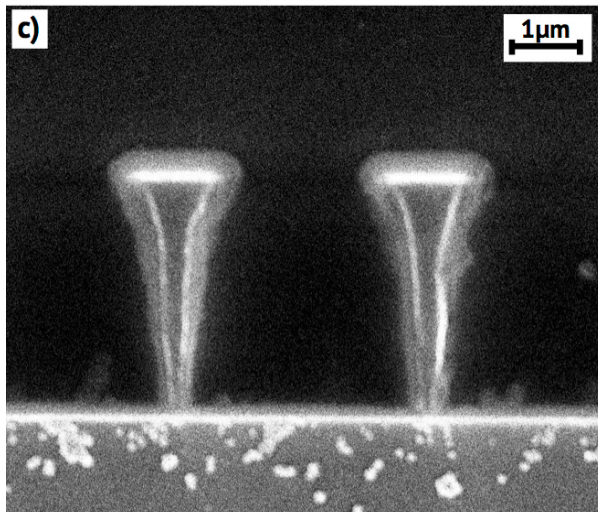
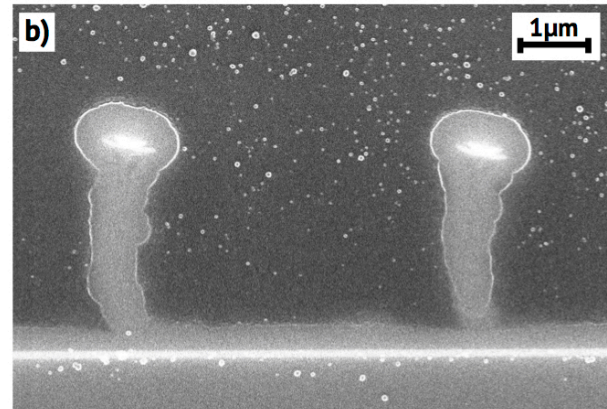
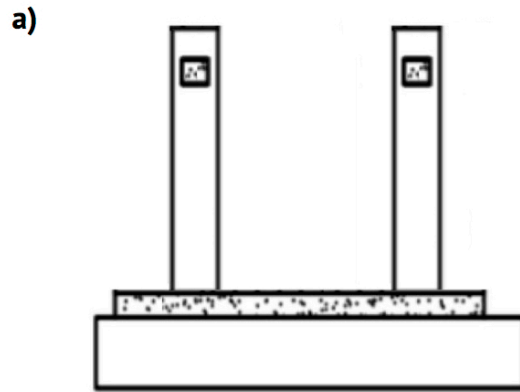
- ✓ Increase SNR
- ✓ Improve lesion detectability
- ✓ Reduce scanning time or radiotracer activity by an amount proportional to the SNR gain
- ✓ Thereby increasing patient throughput or reducing patient radiation dose.

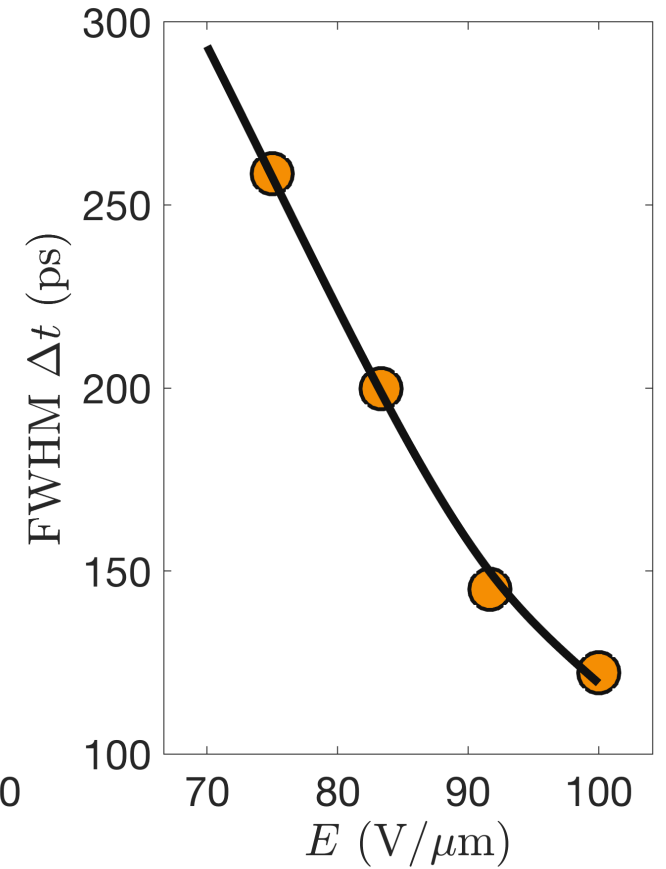
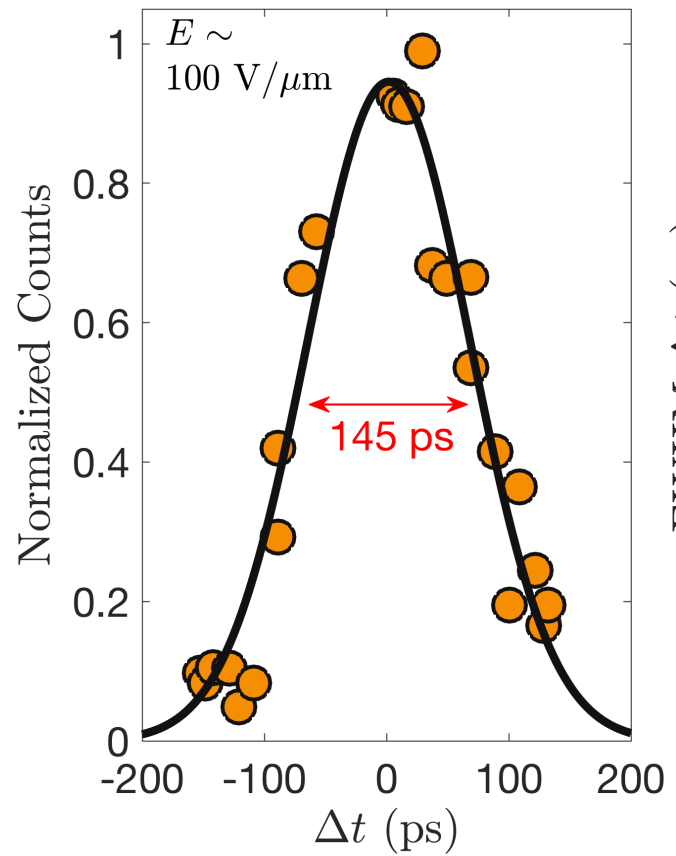
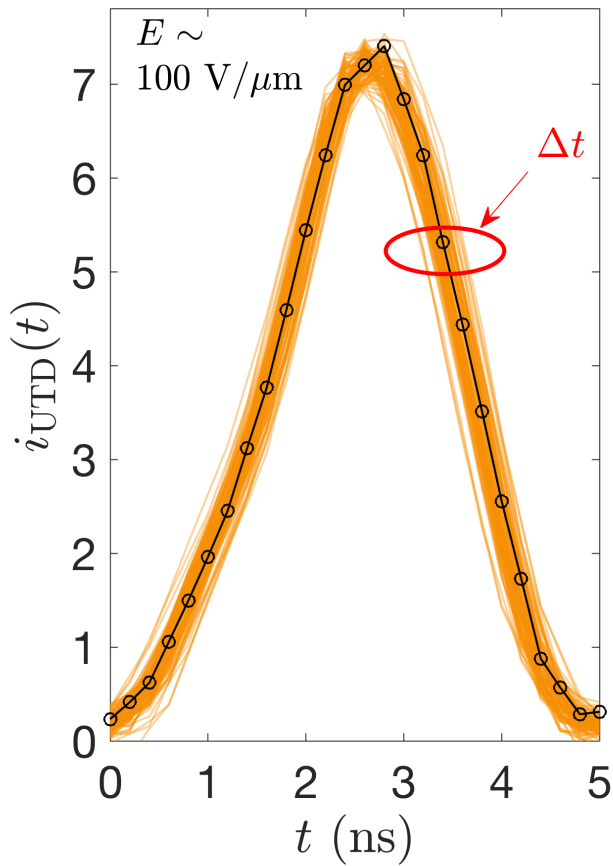
$$\frac{\text{SNR}_{\text{TOF}}}{\text{SNR}_{\text{Non-TOF}}} = \sqrt{\frac{D}{\Delta x}} = \sqrt{\frac{2D}{c \cdot \Delta t}}$$



X. Yang et al, *Phys. Med. Biol.* 58 (2013).

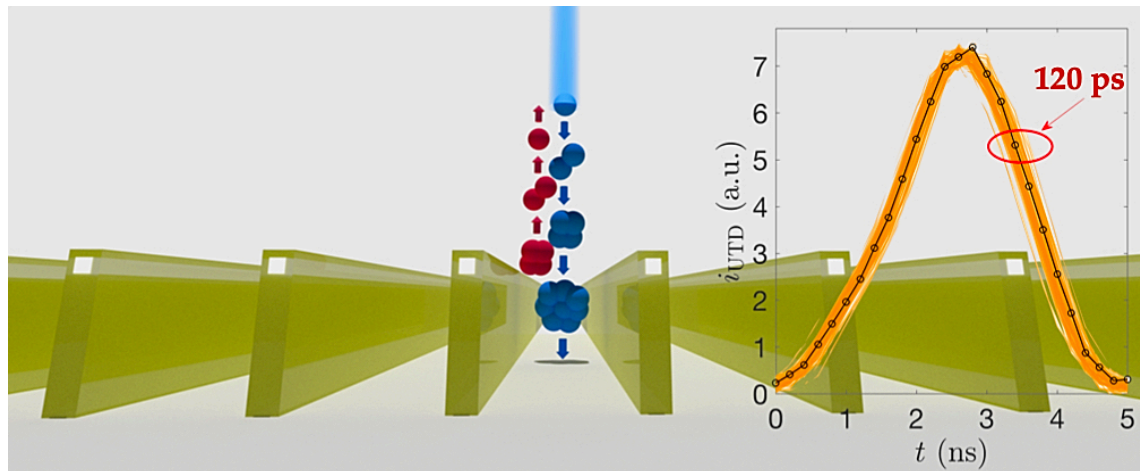




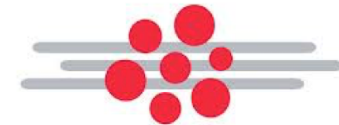




- Amorphous Selenium has tremendous potential as high-sensitivity, large-area, and low cost radiation detector.
- We have reinvented the detector structure using multi-well pixel geometry (with embedded micro- and nano-scale Frisch grids) to obtain avalanche gain and picosecond timing resolution.



- Prof. Wei Zhao
- PhD Students
  - Andrew LaBella
  - Atreyo Mukherjee



**Thank you!**  
**Questions?**